



# Quantitative Ultrasound Computed Tomography using phase-insensitive pyroelectric detectors

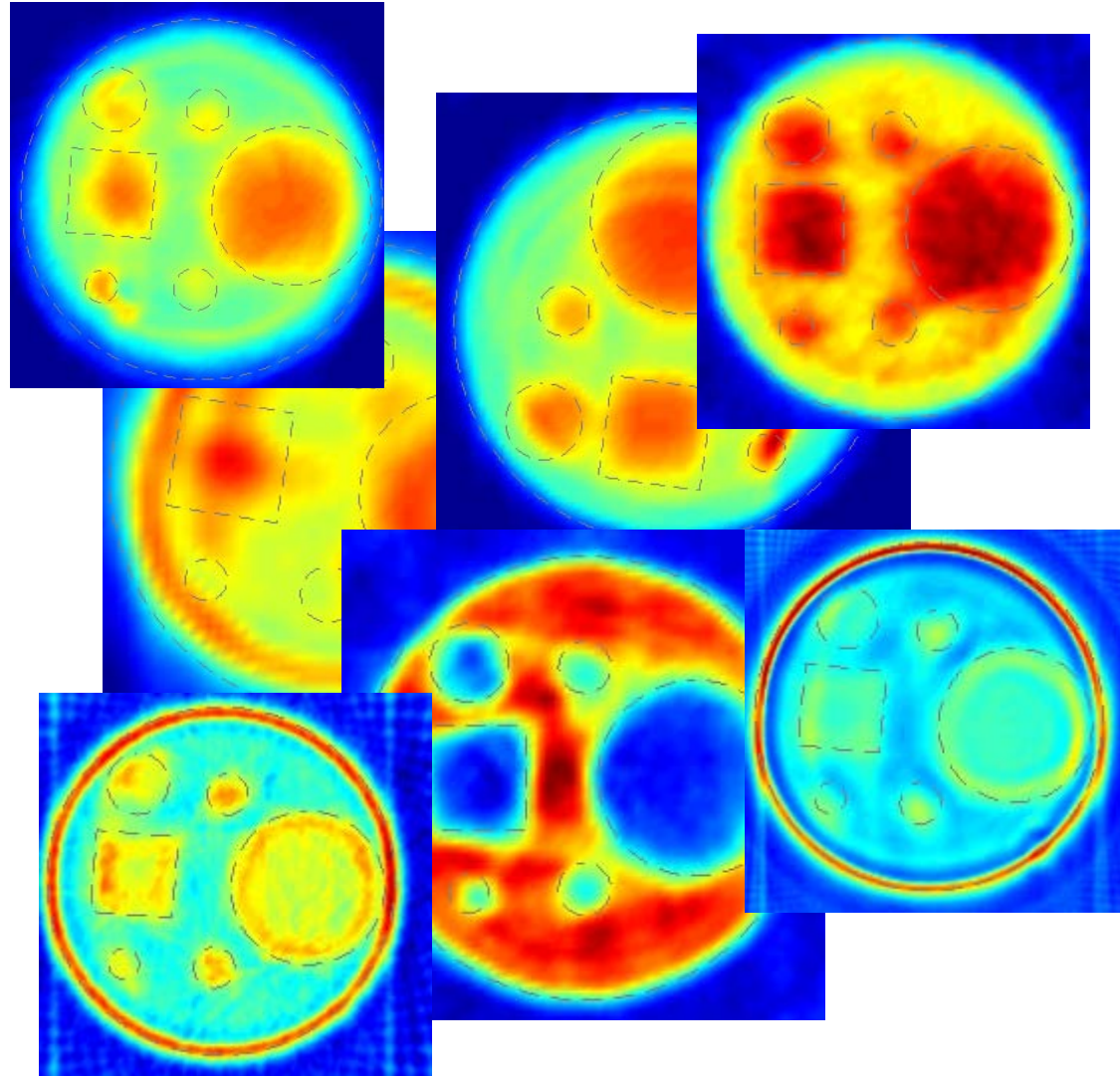
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# Presentation Content

- Motivation
- PI detectors
- UCT System design
- Results
- Summary



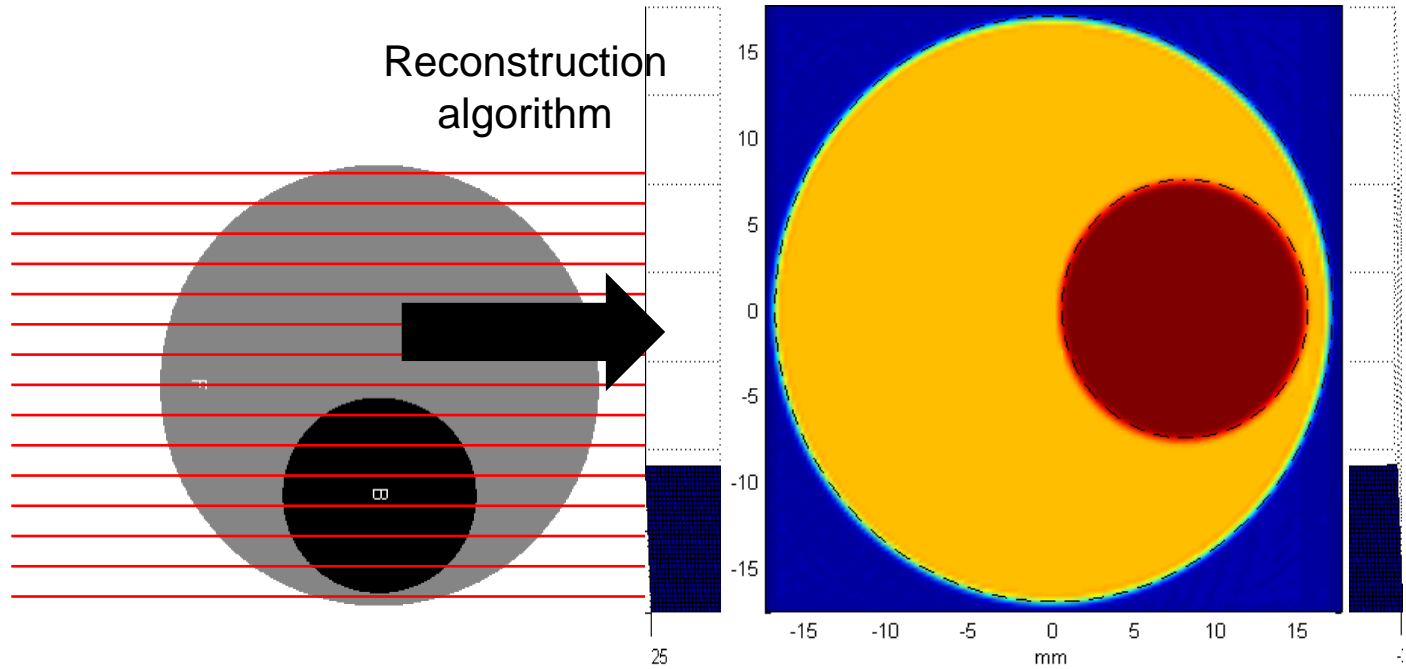
# Motivation

- Ultrasonic Computed Tomography (UCT) is being investigated for whole breast applications;
- Reconstructions are strongly affected by artefacts, particularly when based on ultrasound attenuation of tissue;
- These artefacts arise due to the nature of the detectors used, in particular that they are ***phase-sensitive***;
- In the 1980's, ***phase-insensitive*** detectors based on Cadmium Sulphide acoustoelectric sensors (1980s) seemed to show promise, but were too insensitive;
- This presentation describes ***phase-insensitive*** detectors that exploit the pyroelectric effect in a thin polymer and their application to UCT.

# Computed Tomography (CT)

## Projections

- 

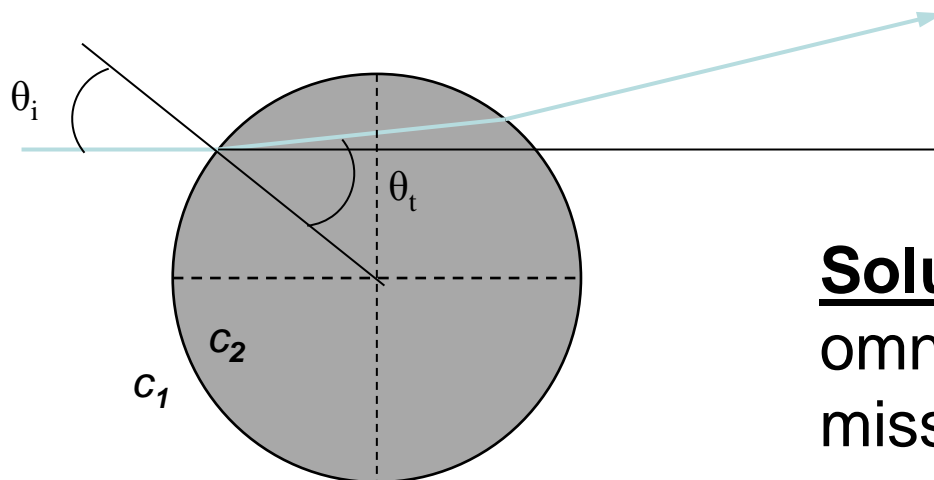


## 2-dimensional image

- Characteristic properties of biological tissues

Speed of sound [m/s]	<i>Fat</i>	<i>Breat fibroglandular tissue</i>	<i>Fibroadenoma</i>	<i>Carcinoma</i>	<i>Cyst</i>
Wiskins <i>et al.</i> 2011	1430 -1460	1550 -1575	1550 -1585	1585 -1630	1520-1540

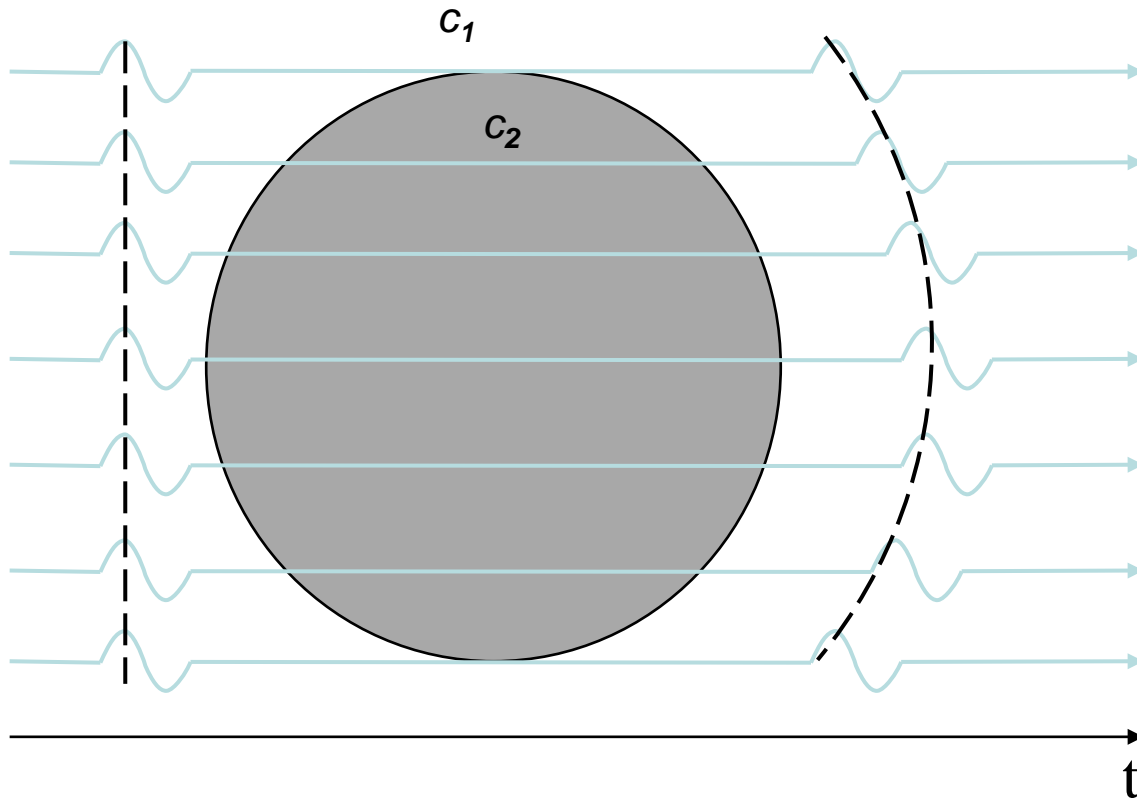
- Refraction of ultrasonic wave-fronts



**Snell's law**

**Solution:** need a large omnidirectional sensor to avoid missing refracted radiation

- Distortion of travelling acoustic wave-fronts



$$C_2 > C_1$$

Acoustic plane-waves

**Solution:** need a phase-insensitive (PI) detector

Biological tissue	$\alpha$ (dB cm <sup>-1</sup> ) 1 MHz	$\alpha$ (dB cm <sup>-1</sup> ) 2.5 MHz	Speed of sound (ms <sup>-1</sup> )
Subcutaneous fat	0.89	1.71	1470
Internal fat	0.92	1.8	1470
High attenuation tumour	0.92	<u>3.2</u>	1549
Cyst	0.06	0.38	1569
Glandular parenchyma	1.02	2.94	1515

*Duric et al. Development of ultrasound tomography for breast imaging, Medical Physics, 32 (5), 2005.*

# Phase-insensitive (PI) detectors

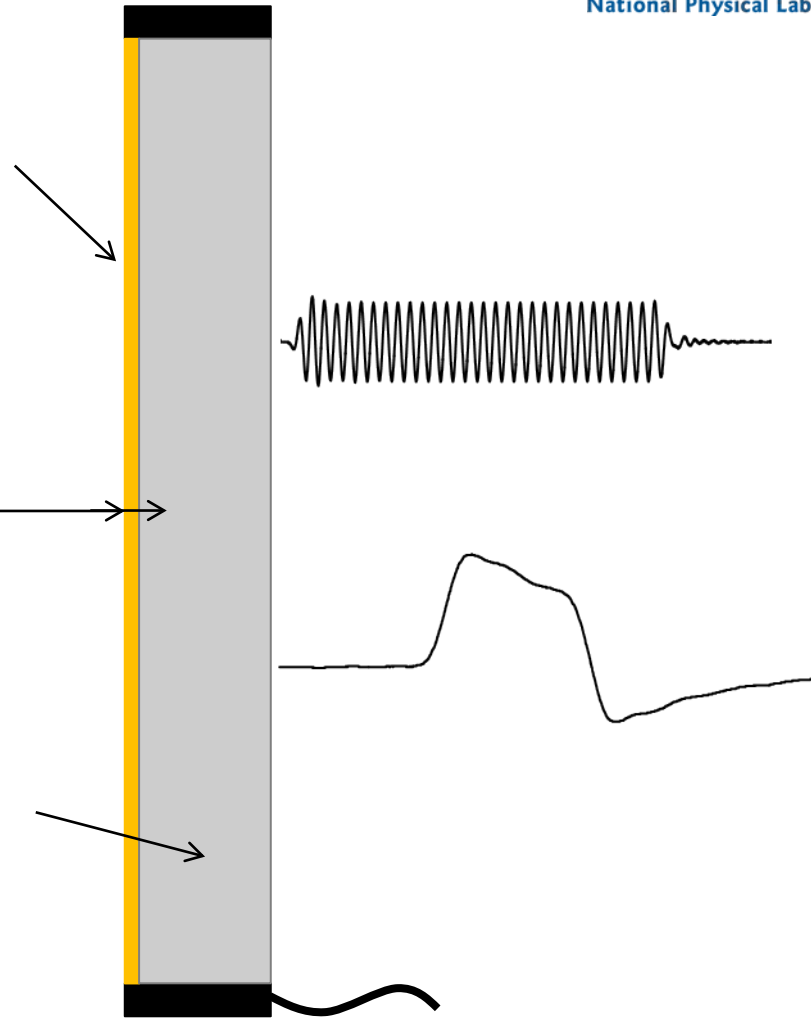


# Pyroelectric Detection

PVdF Layer with gold contacts  
(~110  $\mu\text{m}$ )



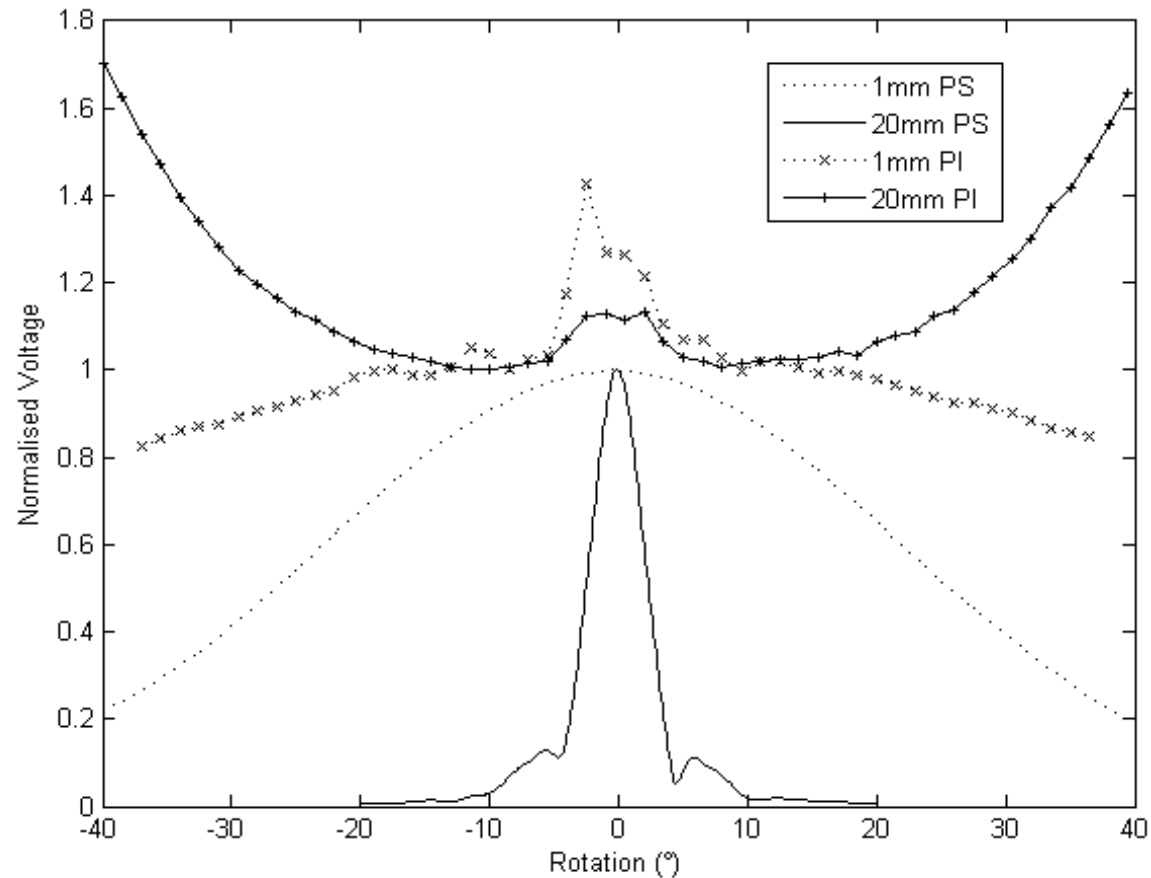
Highly ultrasonically absorbent  
backing layer (~10 mm)



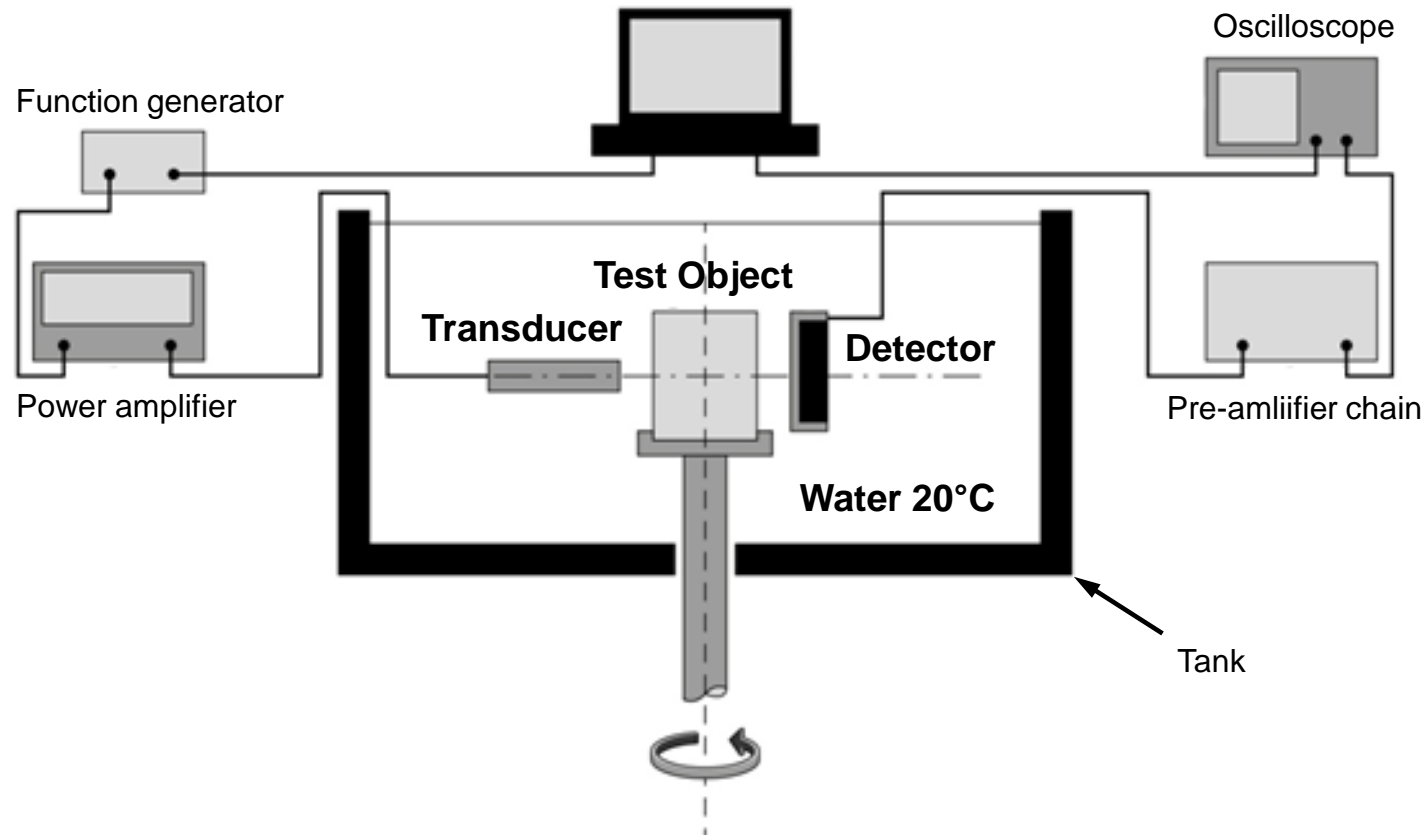
B. Zeqiri, P. N. Gélat, J. Barrie and C.J. Bickley. "A Novel Pyroelectric Method of Determining Ultrasonic Transducer Output Power: Device Concept, Modelling and Preliminary Studies", IEEE Trans. Ultrason., Ferroelectr., Freq. Contr., Vol. 54, No. 11, 2318-2330, 2007.

# Directional Response

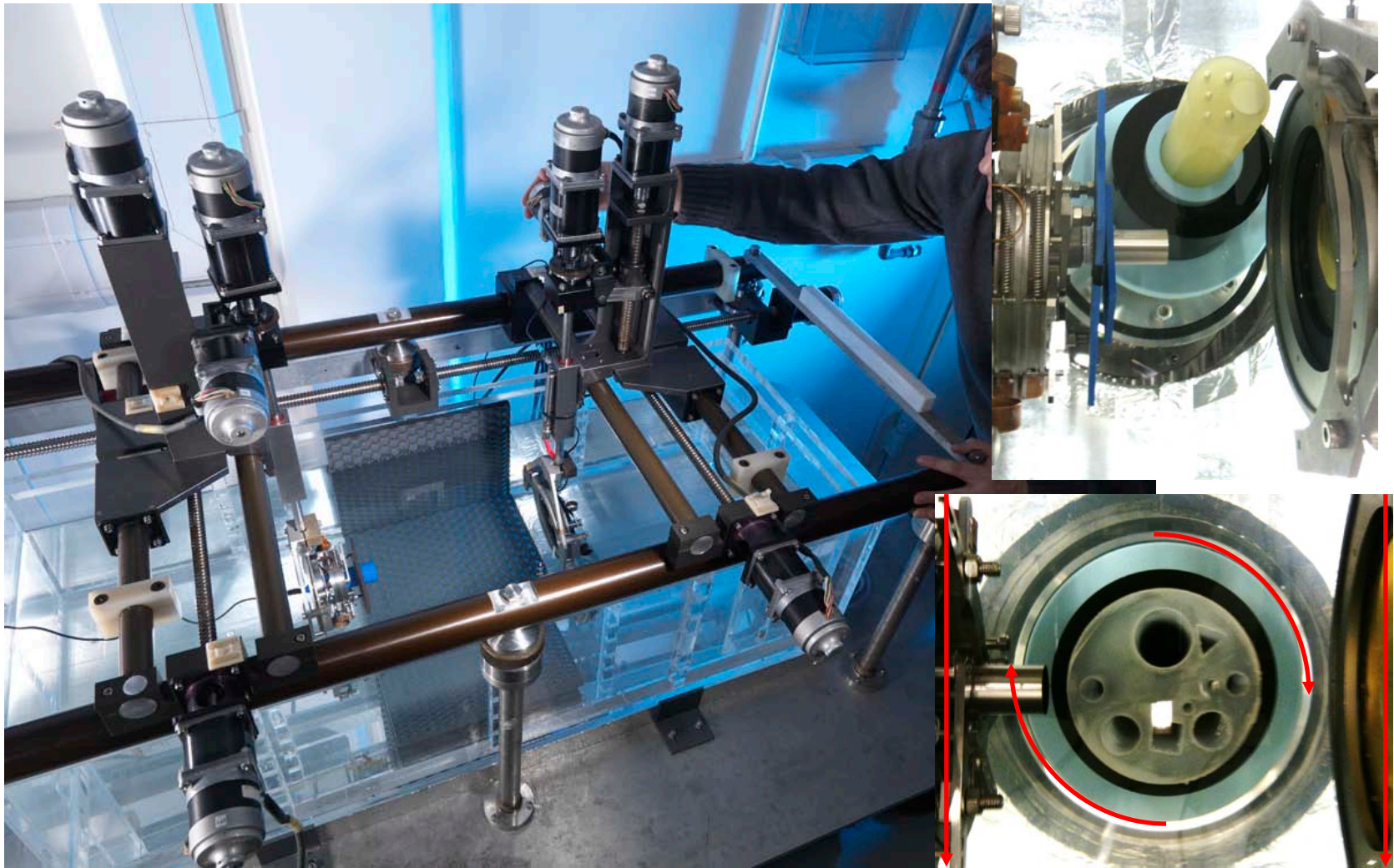
# PI, PS comparison for two detector apertures



# UCT scanning platform

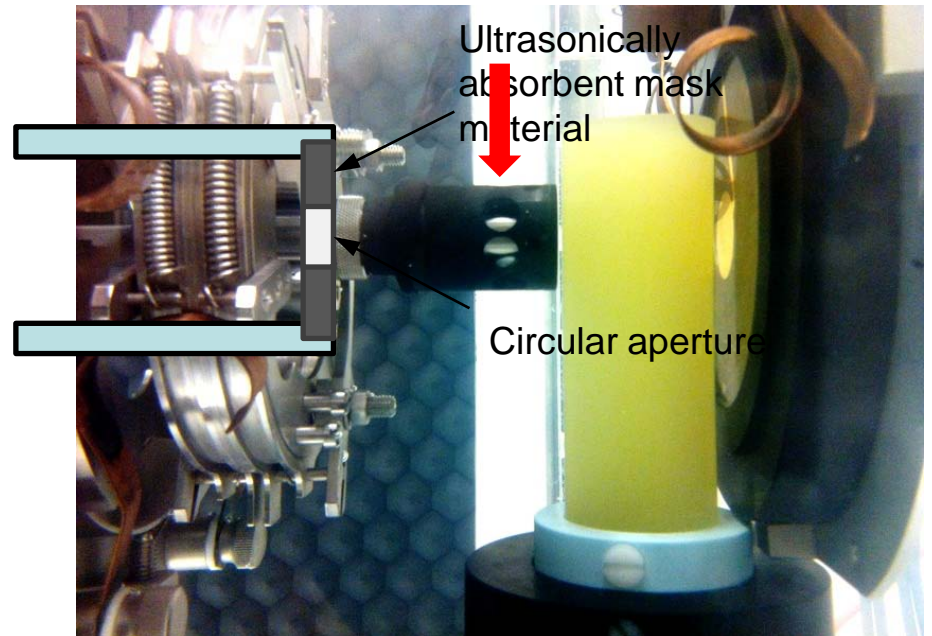
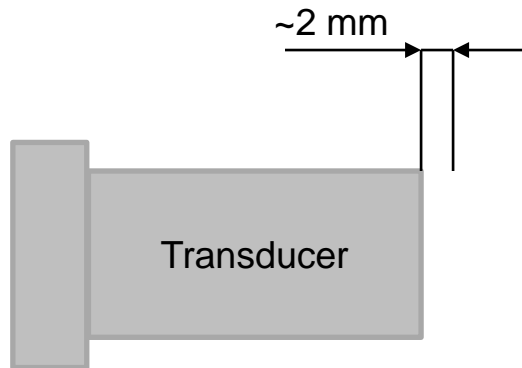


# Pyroelectric UCT System

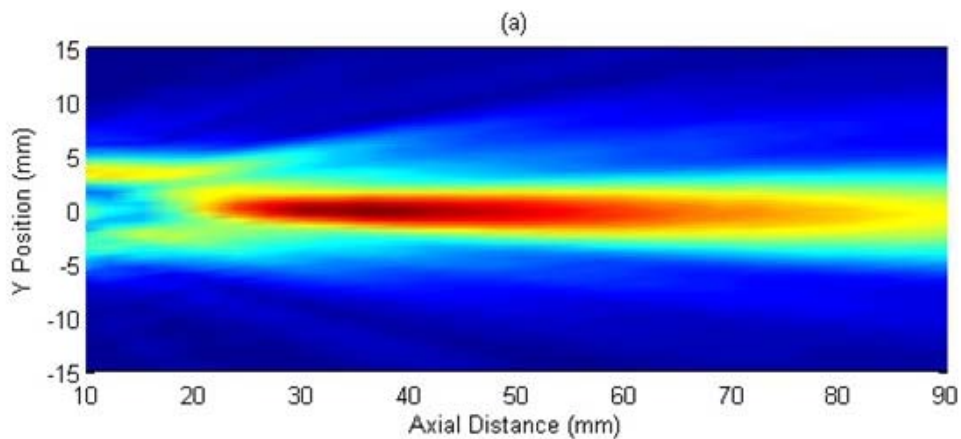


# Collimating the acoustic field

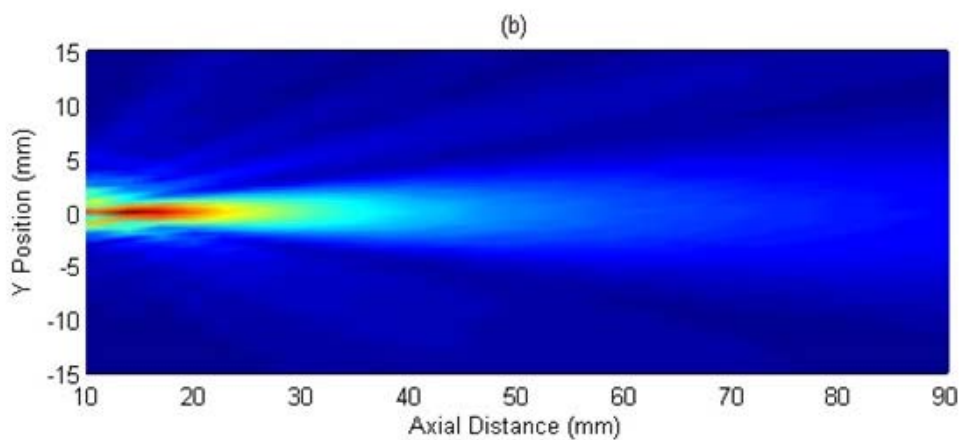
## Collimating mask



## Measurement of the acoustic pressure distribution



- Transducer alone  $\Phi = 12.7\text{mm}$ ;
- **-6 dB Beam-width  $\approx 8\text{ mm}$**



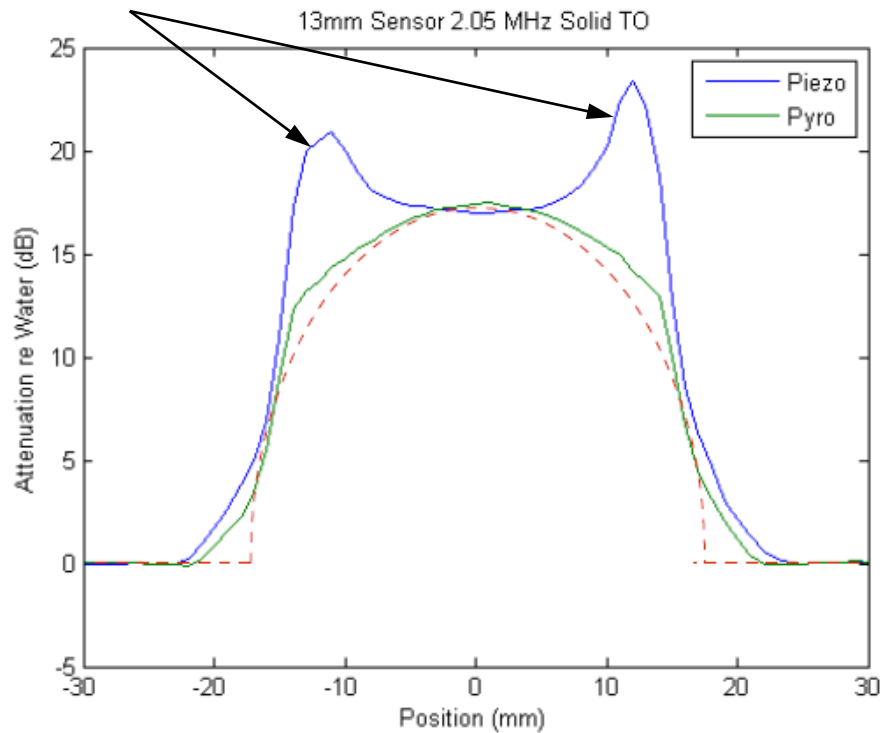
- Masked transducer - mask,  $\Phi = 6\text{ mm}$ ;
- **-6 dB Beam-width  $\approx 3\text{ mm}$**



# Results: projections

# PS vs PI detector responses

Phase cancellation



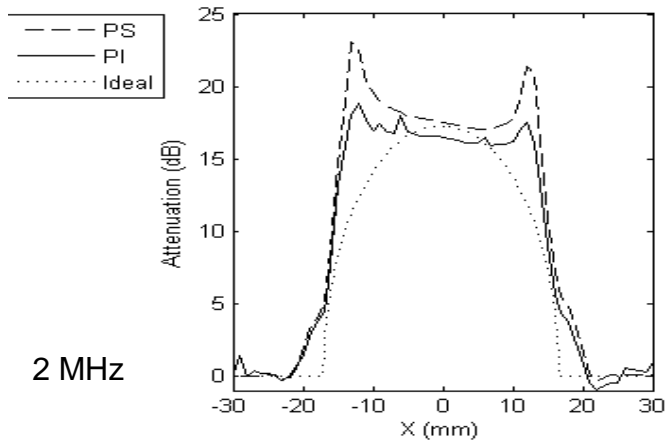
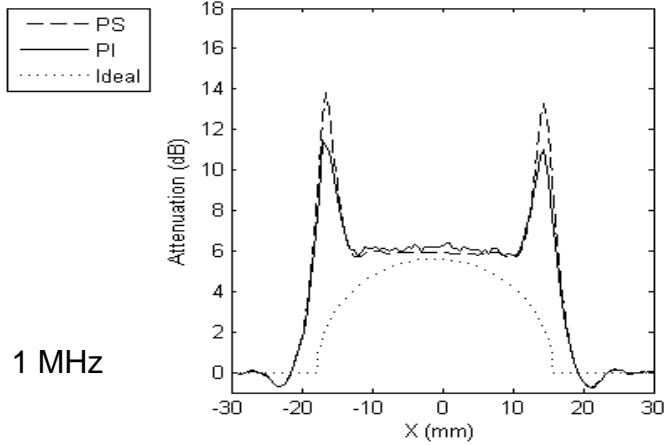
Experimentally derived projection

Homogeneous Test Object



# Results – homogeneous Test Object

4 mm Sensor

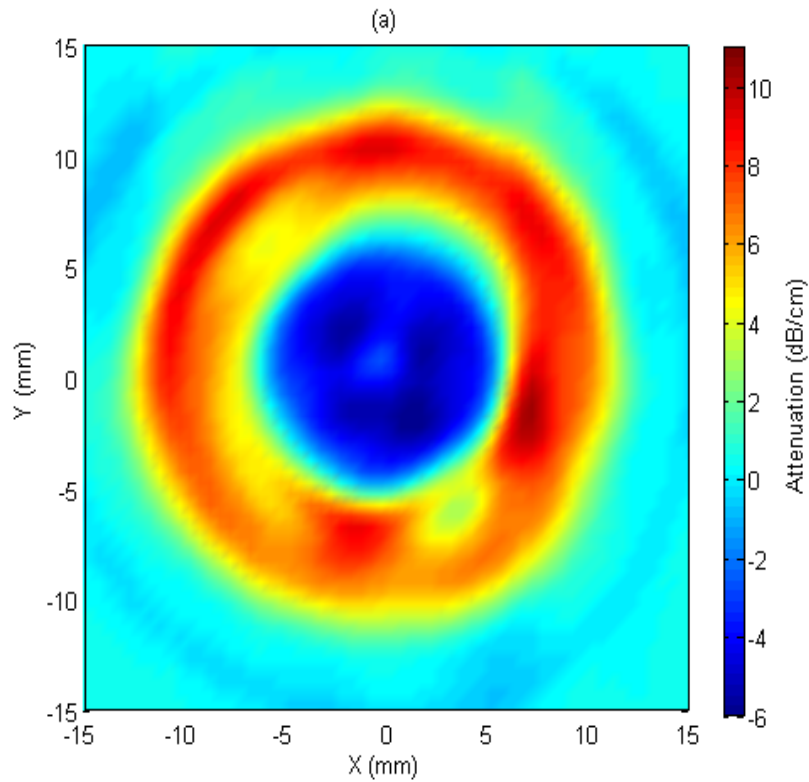


Attenuation (dB)

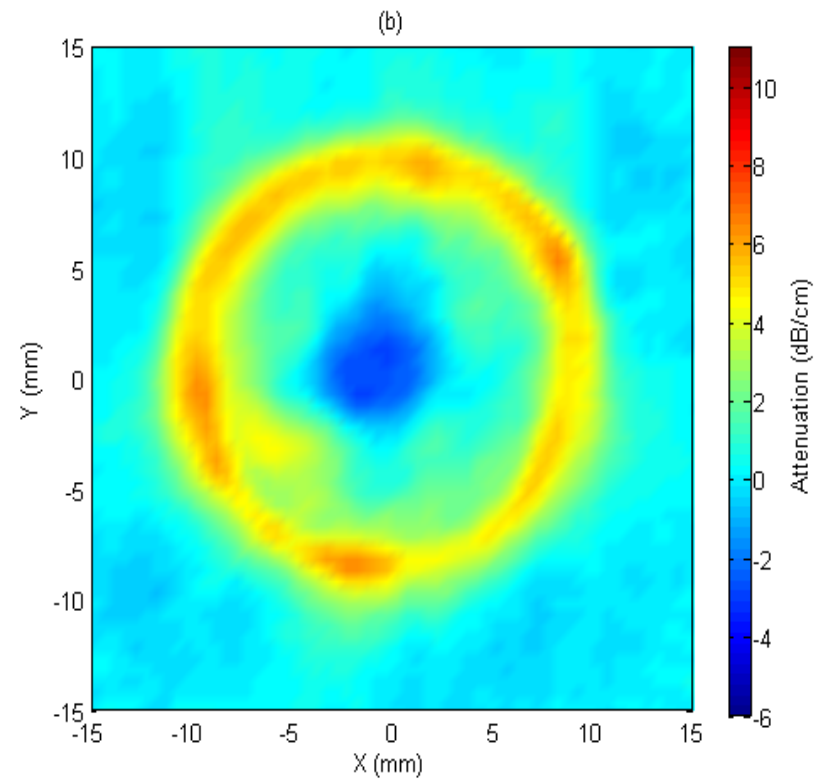
# Results: UCT reconstructions

# Water-filled, thin-walled tube (PETG – 0.38 mm and O/D 20.68 mm).

PS



PI



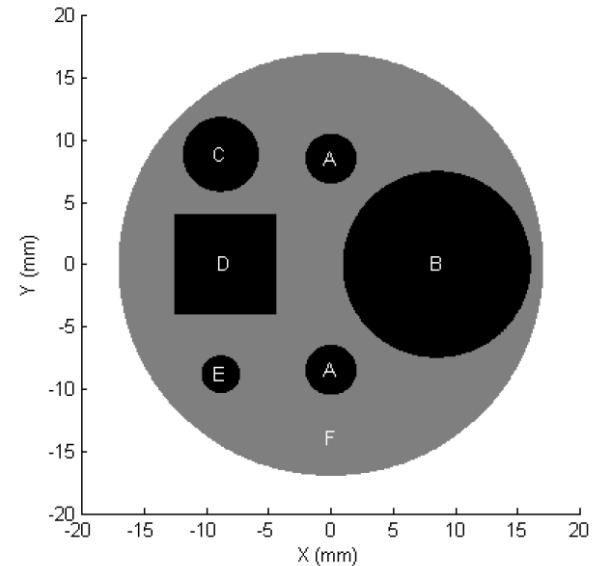
## Experimental conditions



- Plane-piston transducer  $\Phi = 12.7\text{mm}$ , @ 2.05 MHz;
- Detector diameter: 13mm;
- Test Object – Detector: 18mm;
- Two-phase polyurethane Test Object:



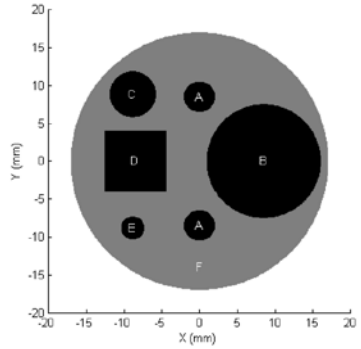
Test Object

Polyurethane properties



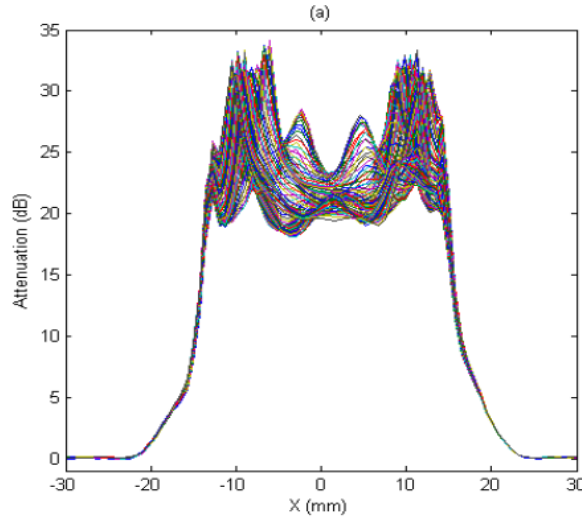
Material type	Component of TO	Sound speed (m/s)	Attenuation coefficient (dB/cm)
<b>Shore A=35</b> 	Background matrix	1538*	5.1 (@ 2.05 MHz)
<b>Shore A=55</b> 	Inserts	1567*	7.5 (@ 2.05 MHz)

\* Speed of sound in water at 20 °C is 1482.4 m/s

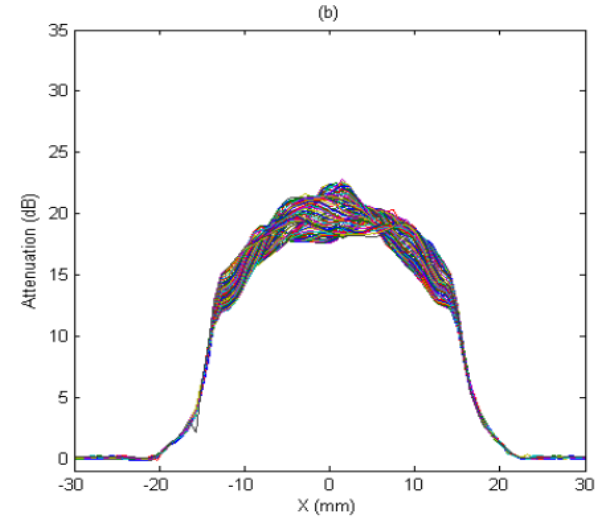


Projections

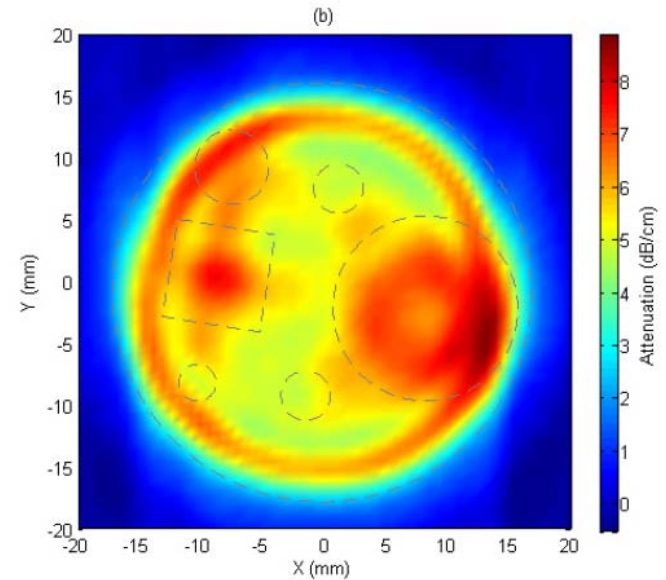
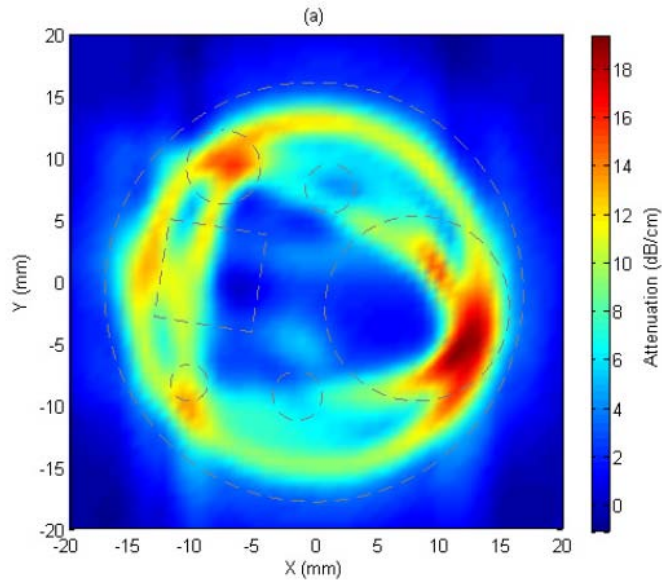
Piezoelectric - PS

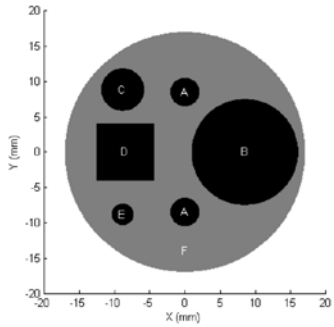


Pyroelectric - PI

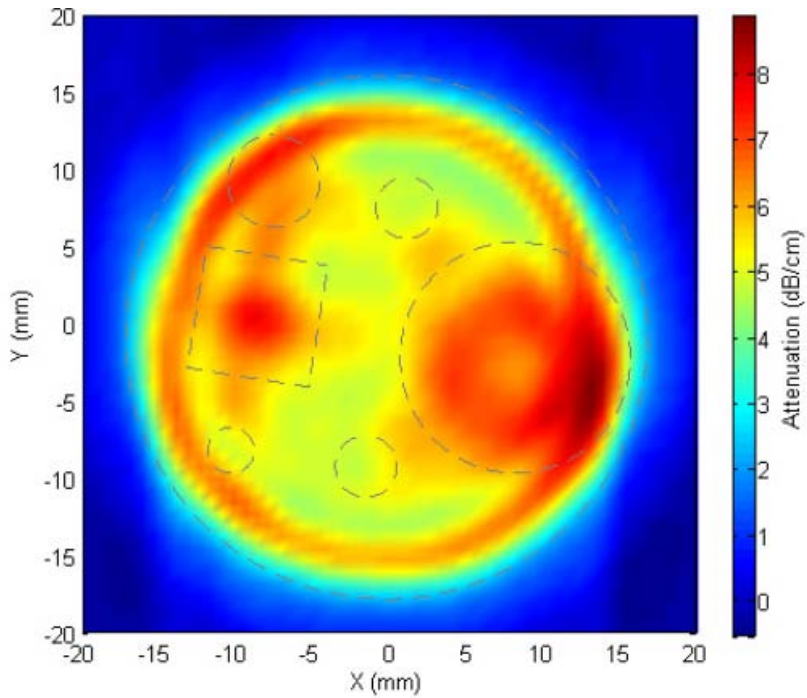


UCT  
Reconstructions



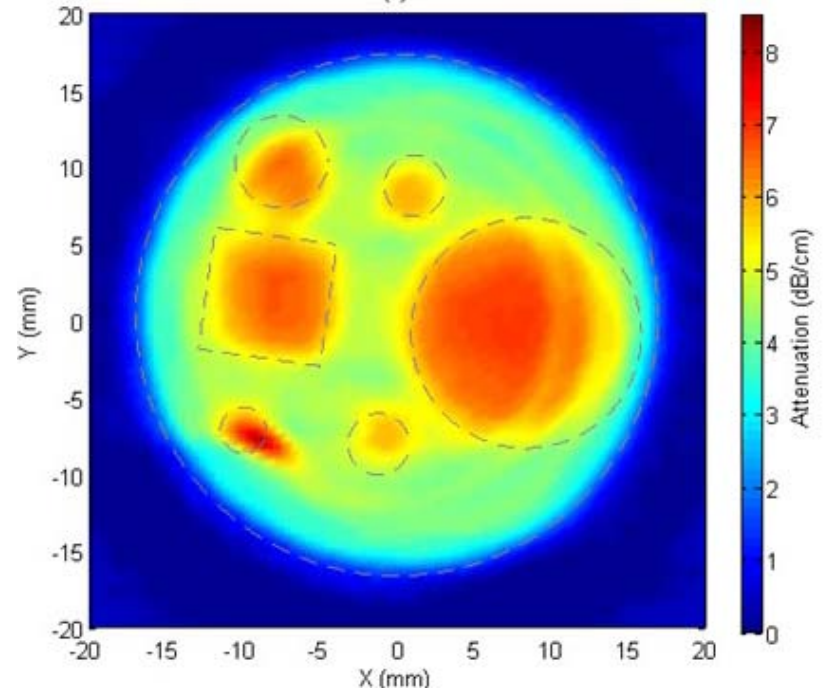


## NO MASK - PI



- Transducer  $\Phi = 12.7$  mm;
- Sensor  $\Phi = 13$  mm

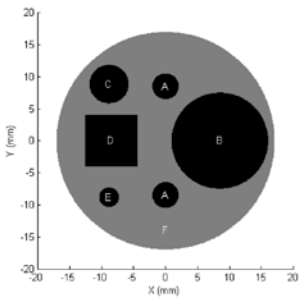
## MASK - PI



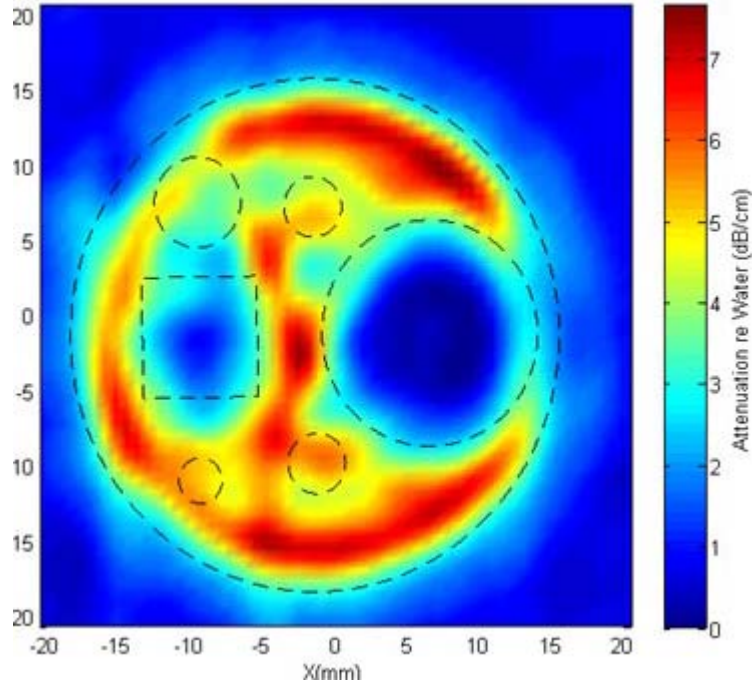
- Transducer + 6 mm  $\Phi$  mask;
- Sensor  $\Phi = 20$  mm



# Water-filled Test Object

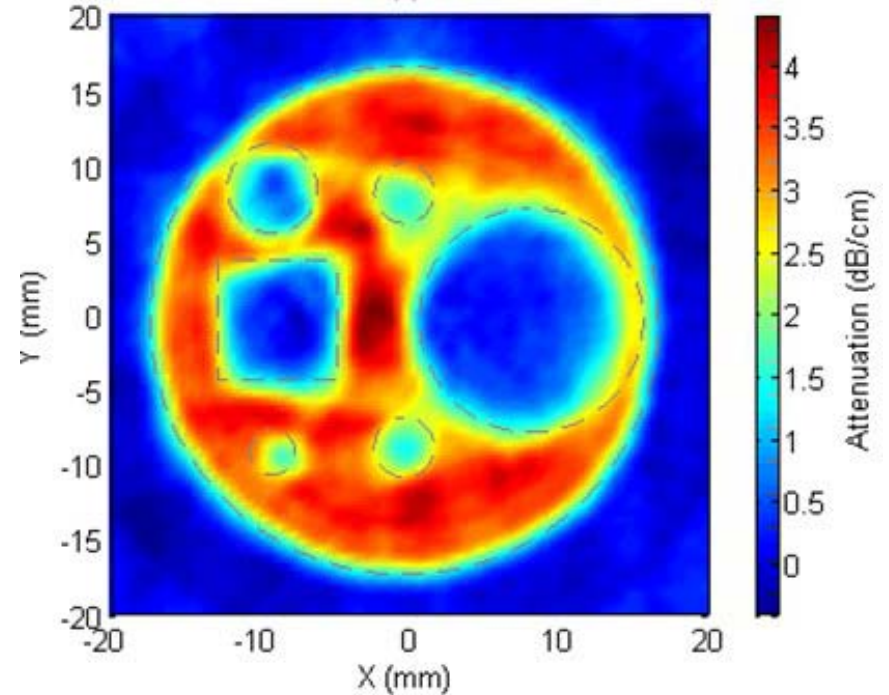


## NO MASK - PI



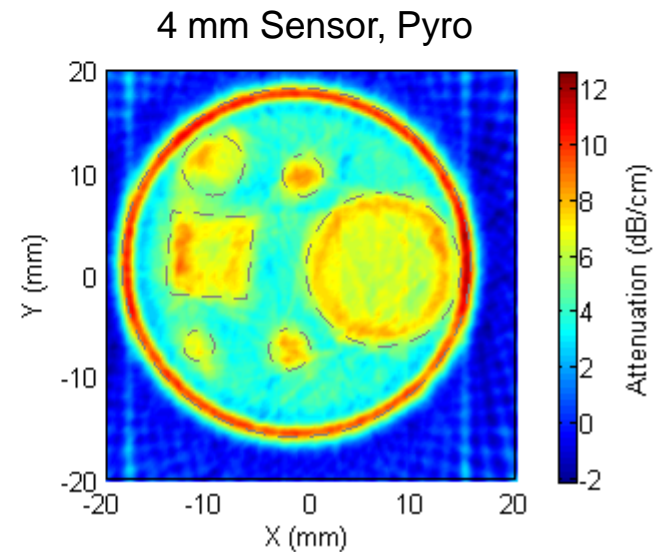
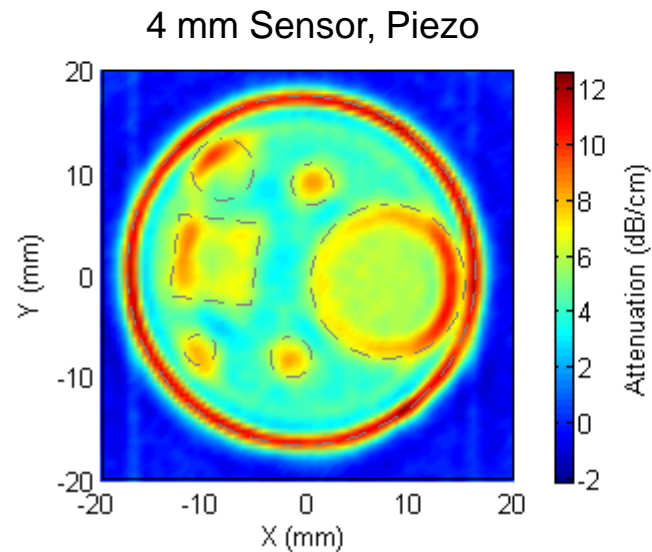
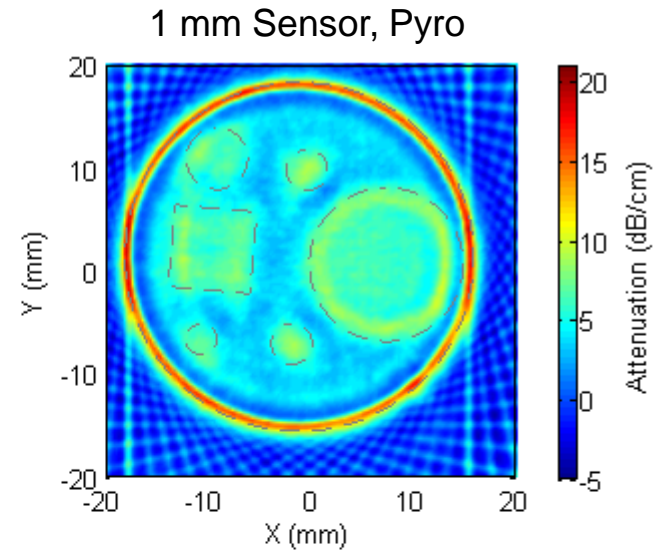
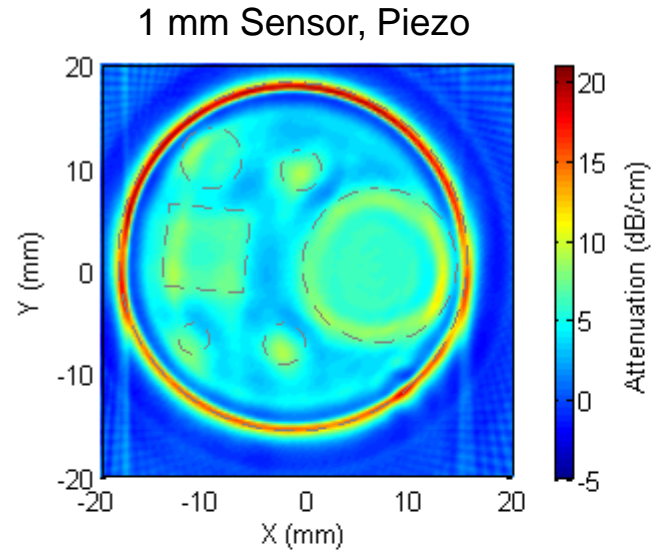
- Transducer  $\Phi = 12.7$  mm;
- Detector  $\Phi = 13$  mm

## MASK - PI



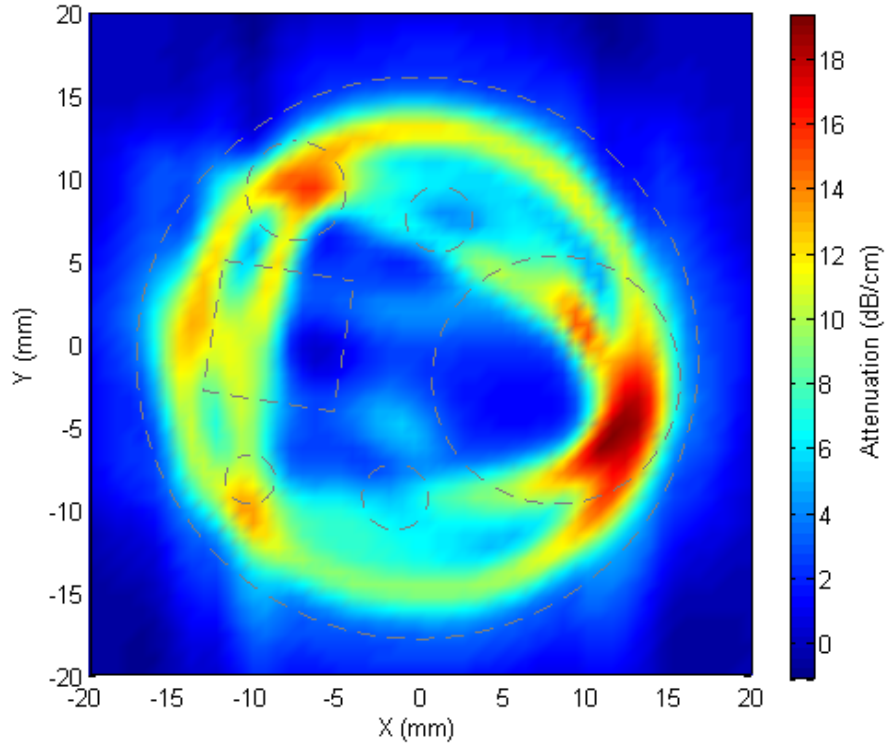
- Transducer + Mask, 6 mm  $\Phi$ ;
- Detector  $\Phi = 20$  mm

# Small area detectors: masked transducer



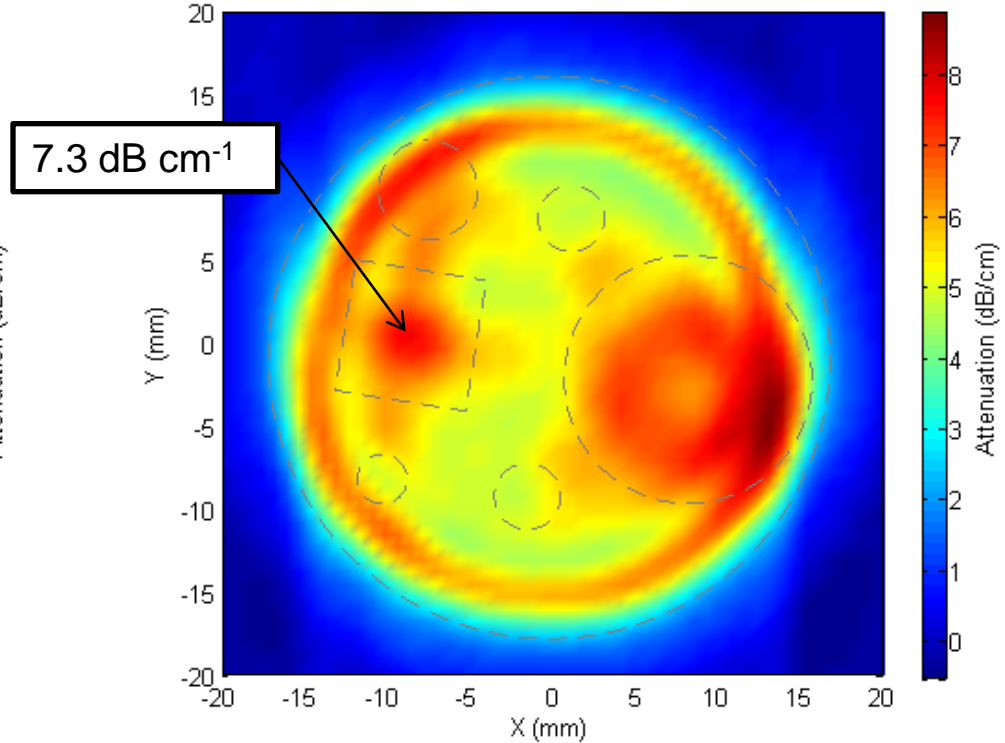
# Quantitative analysis

## Piezo (PS)



*2.05 MHz 12.7 mm transducer  
13 mm sensor*

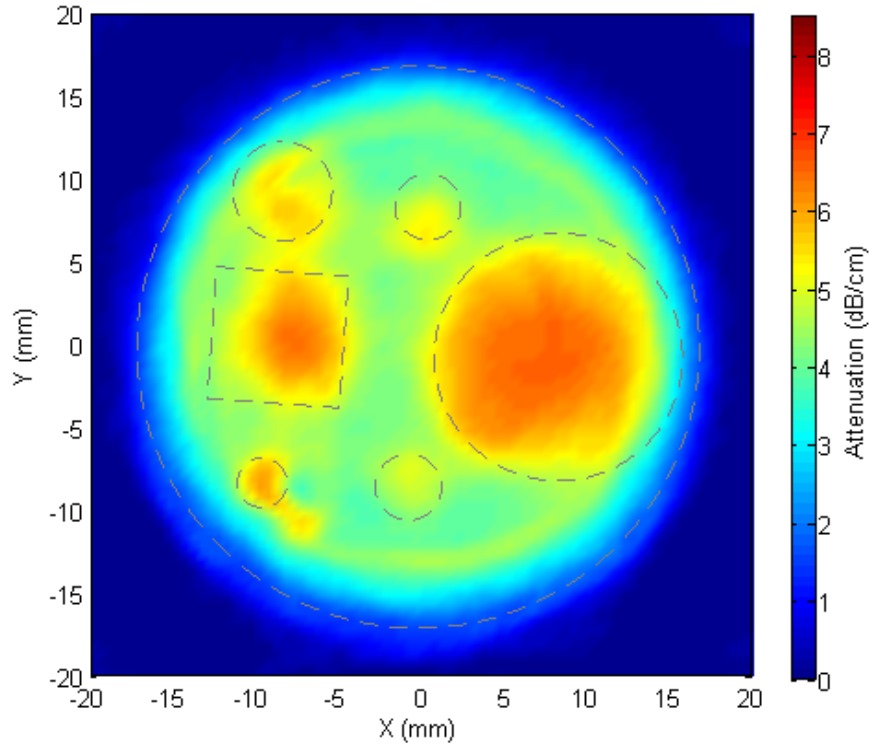
## Pyro (PI)



Rest of inserts: between  $5.8$  and  $6.6 \text{ dB cm}^{-1}$   
***Actual attenuation =  $7.5 \text{ dB cm}^{-1}$***

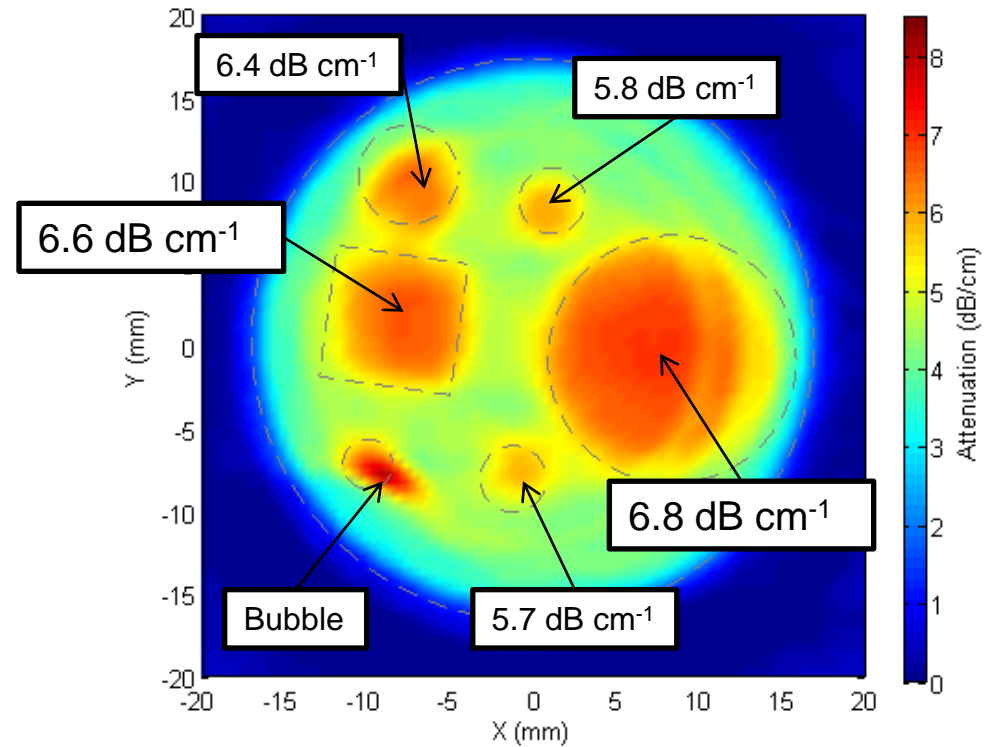
# Masked transducer

## 8 mm Mask, Pyro



*2.03 MHz 12.7 mm transducer  
20 mm detector*

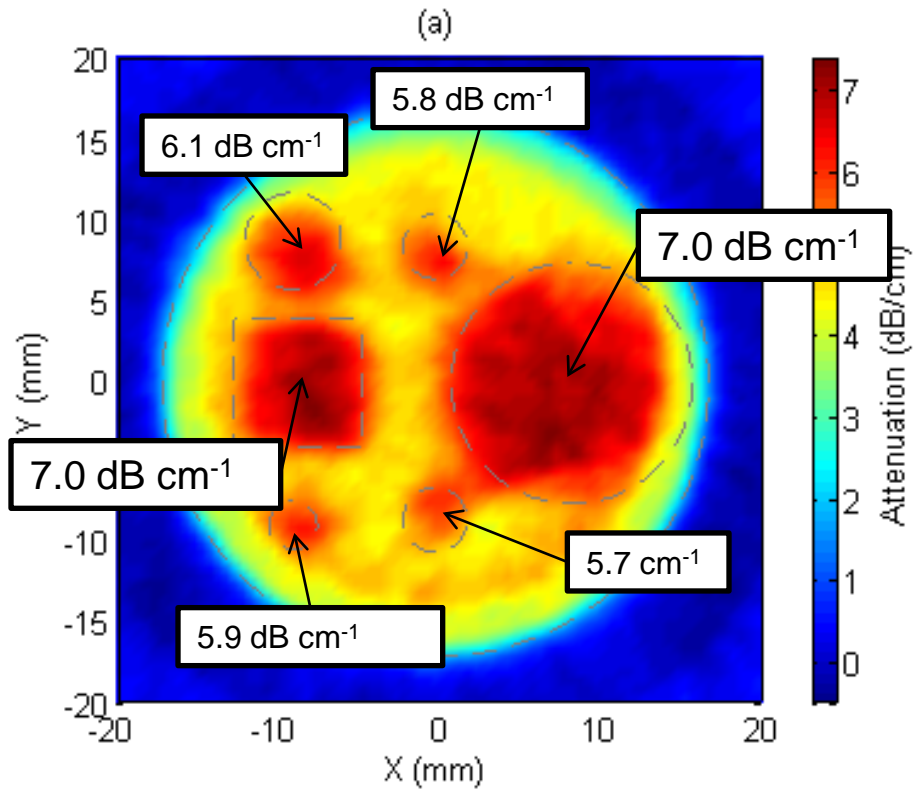
## 6 mm Mask, Pyro



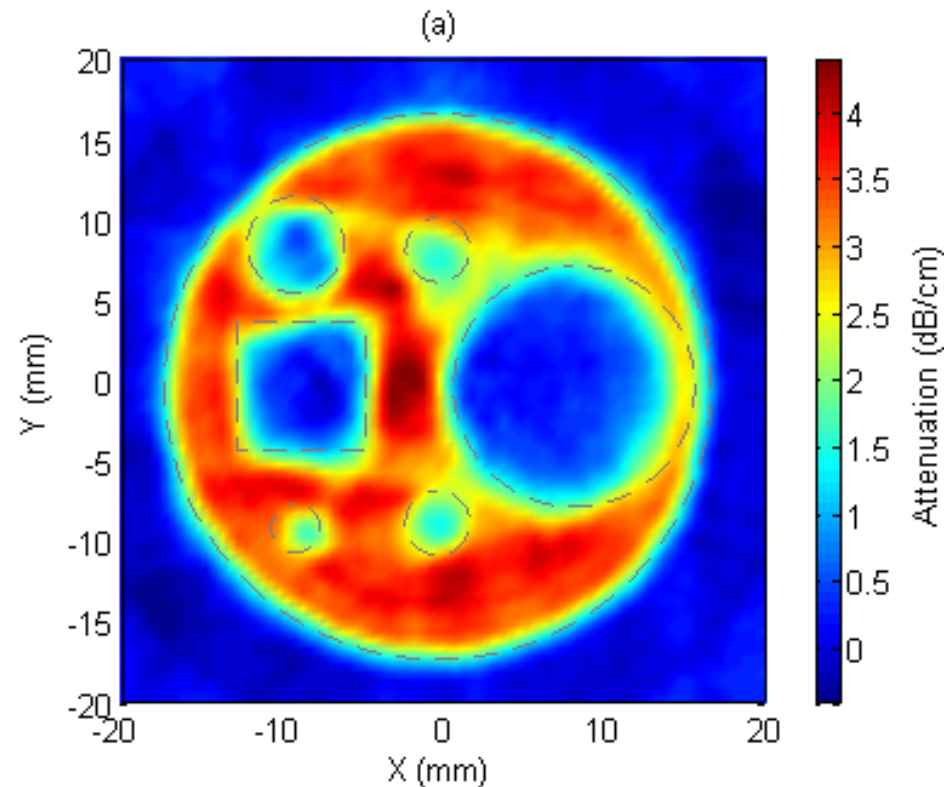
***Actual attenuation = 7.5 dB cm<sup>-1</sup>***

# 6 mm mask, 20 mm sensor

## Two-phase Test Object



## Water-filled

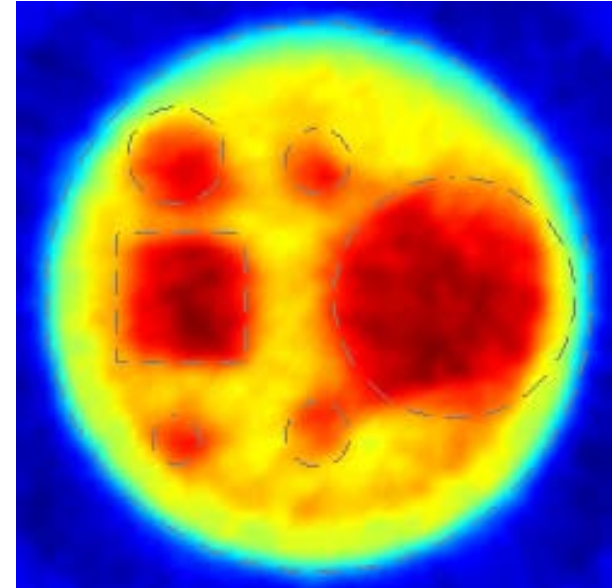


***Actual attenuation = 7.5 dB cm<sup>-1</sup>***

# Summary

- Phase-insensitive (PI) sensors exploiting the pyroelectric effect have been used to reduce UCT artefacts;
- Artefacts arise due to refraction and phase-cancellation;
- PI sensor response is weakly dependent on direction;
- The need for large area PI receivers has been confirmed, the required spatial resolution being produced through the applied acoustic field;
- The PI sensors are non-optimized - changes in sensor design will be needed to boost sensitivity and to improve sensor response time;
- The research has been submitted for publication within **Phys. Med. Biol.**, “*Quantitative ultrasonic computed tomography using phase-insensitive pyroelectric detectors*”.

# Summary



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## Acknowledgements

*Christian Baker, Melissa Mather, Giuseppe Alosa, Mark Hodnett*